

## Improving cell infiltration and visualization of synthetic scaffolds for osteochondral defect repair



### INTRODUCTION

Osteochondral defects affect over 60% of patients that undergo knee surgery and Bilateral osteochondral defect repair was previously performed in an *in vivo* rabbit model to present a major health and mobility concern [1]. These defects are characterized by validate the scaffold. Four groups were tested: damage to both the articular cartilage and underlying subchondral bone, which often result Empty defect (control) from either acute trauma, bone disorders, or long-term degeneration [2]. Current defec Acellular scaffold (only treatments include microfracture and tissue graft transplant, but can lead to additional PLLA scaffold – no cells) complications for patients, such as fibrocartilage formation or donor tissue complexities [3]. Mesenchymal Stem Cell Thus, tissue engineering represents an exciting alternative. Using knowledge of cell and (MSC) seeded scaffold embryonic differentiation, we designed a synthetic scaffold that can support osteo- and (800K cells/scaffold) chondrogenic cell growth and tissue formation. Pre-differentiated scaffold 4 (MSC-seeded + 14 days Small Pores Large Pores of pre-differentiation in biphasic bioreactor)



### **SOLUTION: A PLLA GRADIENT POROUS SCAFFOLD MADE WITH THERMALLY INDUCED PHASE SEPARATION**

To create a scaffold with a gradient of small to large pore sizes, we used a method known To achieve a more robust infiltration of cells into the scaffolds, we first seeded with Vocal Fold as Thermally Induced Phase Separation (TIPS). In a ternary solution of 4% wt PLLA in Fibroblasts (VFFs) which have been immortalized to be tissue cultured for a long time. On the 87/13% wt/wt dioxane/water, opposite sides are exposed to different thermal histories or day of seeding, cells are detached from flasks/plates and split to be resuspended (800k cells/40 cooling rates. As a result, the PLLA solution forms a controlled pore size gradient scaffold µL/scaffold). Scaffolds are placed on their side in a rubber holder and 20 µLs of cell solution are around ice crystals created by the cooling rates (SCS: Slow Cooling Side - small pores, pipetted onto the surface in two intervals. The solution is left to saturate the scaffold for 15 FCS: Fast Cooling Side – large pores) [4]. The final scaffold has pore sizes of ~70µm on mins, and the process is repeated on the opposite side. We collected scaffolds at D0, 3, and 7. one side that smoothly transition to  $\sim 200 \mu m$  on the other side.



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### **BEYOND IN VIVO VALIDATION OF SCAFFOLD DIFFERENTIATION** AND REPAIR IN RABBIT MODEL OSTEOCHONDRAL DEFECTS



These studies have attained in vivo validation of the scaffold's ability to promote localized osteochondral tissue formation and repair post pre-differentiation. My goal was to generate in vitro validation in the rabbit model that is comparable to *in vitro* data in the human model. We proposed main questions:

> HOW CAN WE SEED THE PLLA SCAFFOLDS SUCH THAT CELLS ARE MORE ROBUSTLY SEEDED THROUGHOUT?

> HOW CAN PRESERVATION OF NON-DECALCIFIED TISSUE SECTIONS **IMPROVE STAINS FOR VISUALIZATION?**

### SEEDING PLLA SCAFFOLDS WITH VOCAL FOLD FIBROBLASTS AND SUBSEQUENT VISUALIZATION



The figures above have been adjusted in ImageJ for enhanced visualization. The blue DAPI fluorescent channel is thresholded to red. Scale bars: 1 mm

sectioned the scaffolds before staining with DAPI to visualize. Trial 5 of our scaffold seeding depicted a most improved and saturated cell infiltration into the scaffold, images not

We performed histological and immunofluorescent stains at the **patellofemoral groove** to attain a more optimal visualization of osteochondral morphology. We opted for cryoembedded samples instead of paraffin-embedded ones to avoid a decalcification process that would remove minerals or other calcified tissues from the sample.





GAGs (cartilage).



Opting for cryo-embedded sections helped to avoid decalcification of samples which allowed for better histological and immunofluorescent staining options for visualization. Usage of cryo-tape helped to preserve tissue and sample structure.



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### **IN VITRO VISUALIZATION OF NATIVE RABBIT KNEE SAMPLES USING HISTOLOGICAL ANALYSIS**

Cryosections of "non-decalcified" native rabbit knees were taken with cryo-tape helping to adhere and preserve tissue structure. The tape was mounted onto fresh slides using 0.75% chitosan in 0.375% acetic acid solution.

Hematoxylin & Eosin (H&E) Hematoxylin (purple): nuclei + GAGs Eosin (pink): cytoplasm + matrix



Scale bar: 100µm

**Toluidine Blue** stains for nuclei +

Calcein Blue stains for minerals in the bone front.

Alizarin Red stains strongly for calcium, representative of bone regions.

Non-Decalcified





Alkaline Phosphatase (AP/ALP) is a major regulator of bone mineralization.

Brightfield



Fluorescent (CY3)



All scale bars unless indicated: 1 mm

### **CONCLUSIONS AND NEXT STEPS**







### Next steps:

- Continuing to seed PLLA scaffolds with VFFs.
- Validating rabbit MSCs to use for PLLA seeding and visualization.
- Testing seeding and post-scaffold repair in larger animal models with regeneration capabilities and anatomy closer to humans (i.e., see left for native pig knee samples).

Scale bars: 1 mm

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