Examining Applicability of MM-LLM-RO to Lung Cancer Segmentation By: Aadit Juneja (W, SEAS '27) PennCl Department of Radiation Oncology, University of Pennsylvania School of Medicine Mentors: Sang Ho Lee, Ying Xiao

Abstract

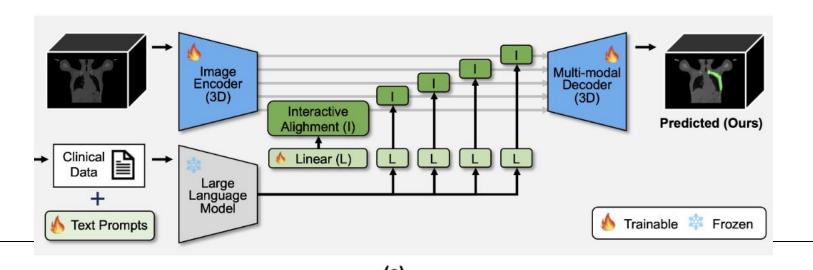
Tumor segmentation from CT scans is a task typically performed by trained professionals in practice. However, the advent of vision language models (VLMs) present an alternative, machinelearning based approach to tackling this task. We explored the usage of MM-LLM-RO, a VLM, in the context of volume contouring for lung cancer. Although no state-of-the-art performances were matched, we discovered modest performances after training the model over a span of 1000 epochs, which took approximately 18 hours on 2 NVIDIA A40 GPUs. The training jobs on these NVIDIA GPUs were submitted largely with the SLURM job submission system on Penn Med's CBICA cluster, though were initially submitted with the SGE method before Penn Med completed the migration.

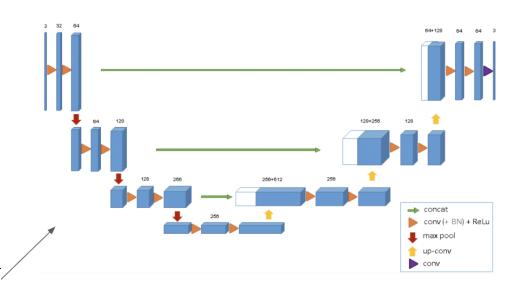
Data preparation took place largely in two parts: text data preparation and CT scan data preparation. Firstly, text data preparation incorporated cleaning a large patient database including information like age, previous conditions, BMI, and other information that would be included by a doctor in a clinical note. I wrote a Python script to turn this information, which was maintained in a spreadsheet-like format, into a natural language clinical note for each patient. I then wrote a new column into the spreadsheet including this note. For the next step, I had to convert the CT scan files, which were provided in Dicom format, to the Nifti format, which proved to be very challenging. Dicom is a 2D format representing cross sections of the scan, meaning 20-25 Dicom files are required to represent one CT scan. However, the Nifti format is one file that represents a 3D image, and thus is more commonly used for inputs to vision language models such as MM-LLM-RO. The script I wrote to convert the file took approximately 4 seconds per sample to run.

ID	HupMrn	A
1	147074469	43.
3	144465112	81.3
4	147022085	66.3
5	155477327	59.
6	147097234	61.
8	147085046	69.
9	147076253	79.2
10	161048153	77.
12	148038616	58.9
13	112082186	66.3
14	144065392	84.4
15	144091029	75.8
16	155834980	78
17	146597038	72.8
18	147031181	73.0
19	14531141	46.9
20	144128256	74.0

Background and Architecture

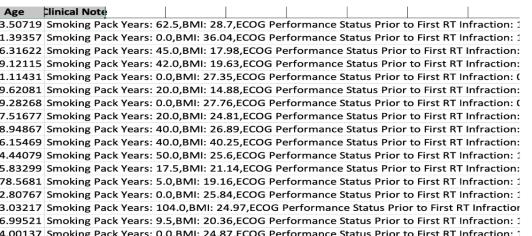
In November 2023, a paper titled MM-LLM-RO was published by Oh et. al. The paper introduced a convolutional U-Net with cross-attention mechanisms to output a segmentation mask on a CT scan predicting the location of a tumor. The model first utilizes downsamples the initial CT scan to a lower dimensional space to learn more meaningful features. Simultaneously, a natural language doctors note is converted into a sequence of tokens via a Llama encoder, with learnable artificial tokens prepending the actual sequence via a prompt tuning mechanism. At each downsampling step, the self-attention adjusted text sequence is projected to the same dimensionality as the current dimensionality of the image sequence via a linear layer, after which cross-attention is conducted between the image and text sequences, which are now of the same dimensionality. This is performed until the CT scan representation reaches the "bottom" of the U-Net architecture in its lowest dimensionality. Afterwards, the representation is upsampled back up to original dimensionality, with the initial representation during the downsampling phase preattention is concatenated with this representation as part of a residual layer. Once mapped back to the CT scan representation, softmax is applied to arrive at per-voxel probabilities. The model is trained with a weighted loss combining binary cross entropy and a DICE loss.



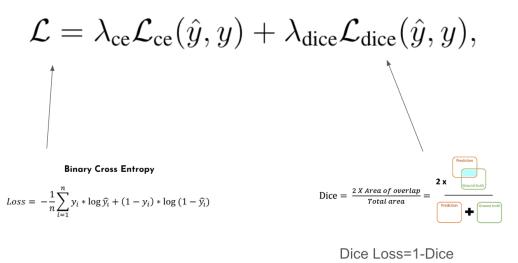


Program: Penn Undergraduate Research Mentoring Program (PURM)

Data Preparation







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			Res	ults
ID 100 129 140 177 183 201 365 366 378 444 468	0.589 0.788 0.845 0.855 0.854 0.723 0.87 0.87 0.801 0.272			Mon Aug 5 06:50:34 2024 epoch, loss, mean, ptv, ctv, gtv 60, 1.025, 0.000019, 0.000 65, 0.982, 0.031315, 0.031 70, 0.935, 0.094633, 0.095 75, 0.917, 0.126797, 0.127 80, 0.852, 0.228411, 0.228 85, 0.828, 0.263805, 0.264 90, 0.792, 0.290622, 0.291 95, 0.830, 0.227073, 0.227 100, 0.835, 0.247232, 0.247 105, 0.693, 0.427618, 0.428 110, 0.755, 0.362875, 0.363 115, 0.819, 0.252012, 0.252 120, 0.706, 0.4406319, 0.406 125, 0.706, 0.414761, 0.415 130, 0.729, 0.391443, 0.391 135, 0.712, 0.360358, 0.360
50 524 542 773 791 792 877 878 878 882	0.691 0.74 0.752 0.461 0.557 0.47 0.712 0.728			140, 0.701, 0.372080, 0.372 145, 0.734, 0.325806, 0.326 150, 0.659, 0.429564, 0.430 155, 0.639, 0.438234, 0.438 160, 0.672, 0.420778, 0.421 165, 0.685, 0.375816, 0.376 170, 0.623, 0.440226, 0.440 175, 0.679, 0.389830, 0.390 180, 0.658, 0.403954, 0.404 185, 0.632, 0.426750, 0.427 190, 0.628, 0.450067, 0.450 195, 0.587, 0.502042, 0.502 200, 0.537, 0.534581, 0.535

The left image appears to represent the average IoU and Dice loss score for each of the images in the validation dataset after the model is trained. The right image is a picture of the loss logs over the model's training horizon, indicating decreasing losses over the 1000 epoch training period. Note that not all 1000 epochs are included in this picture due to sizing limitations.

<u>Acknowledgements</u>

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